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An Energy Minimization Reconstruction Algorithm for Multivalued Discrete Tomography

László Varga, Péter Balázs, Antal Nagy

University of Szeged, Hungary Department of Image Processing and Computer Graphics

7 September 2012

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Transmission tomography

- We are interested in the inner structure of some given object.
- We can measure the projections of the object of study (the densities of the object on the path of some projection beams).
- The goal is to reconstruct the original structure from a given set of projections.



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Transmission tomography

• The object of study is represented by a function f(u, v).

$$f: \mathbb{R}^2 \to \mathbb{R} \tag{1}$$

• We take the line integrals of the image (Radon-Transform).

$$[\mathcal{R}f](\alpha,t) = \int_{-\infty}^{\infty} f(t\cos(\alpha) - q\sin(\alpha), t\sin(\alpha) + q\cos(\alpha)) \, dq$$
(2)

• We are looking for an f'(u, v) function that has the same projections as the original f(u, v).

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Discrete Tomography

In discrete tomography we assume that the object of study consists of only a few known materials.

$$f(u,v) \in \{l_1, l_2, \dots, l_c\}$$
(3)

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With this information we can gain accurate reconstructions from only few (say, 2-10) projections.

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Formulation of the reconstruction problem

- We assume a discrete representation of the object of study (i.e., it is represented on an $n \times n$ sized discrete image).
- The projections are given by the integrals of the image along a set of straight lines.





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Formulation of the reconstruction problem

- With this the reconstruction problem can be reformulated a a system of equations **Ax** = **b**, where:
 - **b**, is the vector of *m* projection values,
 - x, represents the vector of the image pixel values,
 - **A**, describes the connection between the image pixels, and the projection values, with all a_{ij} giving the length line segment of the *i*-th projection line in the *j* pixel.
- We will further assume, that the pixel intensities are elements of a predefined set $L = \{l_1, l_2, \dots, l_c\}$.





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Energy function

With the algebraic formulation of the reconstruction algorithm, one can construct an energy function that takes its minima in the correct reconstructions.



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Discretizing term

The part of the energy function responsible for the discretizing can be given in the form

$$g(\mathbf{x}) = \sum_{i=1}^{n^2} g_p(x_i) , \ i \in \{1, 2, \dots, n^2\} ,$$
 (4)

where

$$g_p(z) = \begin{cases} \frac{\left[\left(z-l_{j-1}\right)\cdot\left(z-l_{j}\right)\right]^2}{2\cdot\left(l_j-l_{j-1}\right)^2}, & \text{ha } z \in [l_{j-1}, l_j] \text{ for each} \\ & j \in \{2, \dots, c\}, \\ \text{undefined}, & \text{otherwise.} \end{cases}$$

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Discretizing term

The discretizing term is given as the sum of one-dimensional discretizing functions written on each pixel value, which

- takes a 0 minimum, at the discrete values of *L*,
- and takes high positive values between the desired intensities.



Example of the discretizing function of one pixel with $L = \{0, 0.25, 0.5, 1\}$ expected intensities.

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Basic process of the optimization

- The minimized energy function is basically constructed of two parts:
 - Two convex terms responsible for projection correctness, and "smoothness".
 - A non-convex discretizing term preferring discrete solutions of *L*.

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$$\mathcal{E}_{\mu}(\mathbf{x}) := \frac{1}{2} \cdot \|\mathbf{A}\mathbf{x} - \mathbf{b}\|_{2}^{2} + \frac{\alpha}{2} \cdot \sum_{i=1}^{n^{2}} \sum_{j \in N_{4}(i)} (x_{i} - x_{j})^{2} + \mu \cdot g(\mathbf{x}), \ \mathbf{x} \in [l_{1}, l_{c}]^{n^{2}}$$
(5)

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Basic process of the optimization

- We assume that, the most important part of the energy function is the projection correctness term, and start the optimization with a gradient method as follows:
 - 1 At the beginning we omit discretization.
 - We start running a gradient method from an initial solution.
 - 3 As the projections of the current intermediate solution get closer to the desired ones, we slowly start to increase the weight of the discretization
 - When the iteration does not make significant changes of the results, we stop the process.

The algorithm

Reconstruction Algorithm for Multivalued Discrete Tomography

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Input: A projection matrix, **b** expected projection values, \mathbf{x}^0 initial solution, $\alpha, \mu, \sigma \ge 0$ predefined constants, and *L* list of expected intensities.

- 1: $\lambda \leftarrow$ an upper bound for the largest eigenvalue of the $(\mathbf{A}^T \mathbf{A} + \alpha \cdot \mathbf{S})$ matrix.
- 2: $k \leftarrow 0$
- 3: repeat
- 4: $\mathbf{v} \leftarrow \mathbf{A}^T (\mathbf{A} \mathbf{x}^k \mathbf{b}).$
- 5: $\mathbf{w} \leftarrow S\mathbf{x}^k$
- 6: **for** each $i \in \{1, 2, ..., n^2\}$ **do** 7: $y_i^{k+1} \leftarrow x_i^k - \frac{v_i + \alpha \cdot w_i + \mu \cdot G_{0,\sigma}(v_i) \cdot \nabla g_{\rho}(x_i^k)}{\lambda + \mu}$

$$x_i^{k+1} \leftarrow \begin{cases} I_1, & \text{if } y_i^{k+1} < I_1, \\ y_i^{k+1}, & \text{if } I_1 \le y_i^{k+1} \le I_c, \\ I_c, & \text{if } I_c < y_i^{k+1}. \end{cases}$$

9: end for

8:

- 10: $k \leftarrow k+1$
- 11: until a stopping criterium is met.
- 12: Apply a discretization of \mathbf{x}^k to gain fully discrete results.

The algorithm

Minimization Reconstruction Algorithm for Multivalued Discrete Tomography

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Optimization process

Input: A projection matrix, b expected projection values, \mathbf{x}^0 initial solution, $\alpha, \mu, \sigma > 0$ predefined constants, and L list of expected intensities.

- 1: $\lambda \leftarrow$ an upper bound for the largest eigenvalue of the $(\mathbf{A}^T \mathbf{A} + \alpha \cdot \mathbf{S})$ matrix.
- 2: $k \leftarrow 0$
- 3: repeat

7

8

- 4: $\mathbf{v} \leftarrow \mathbf{A}^T (\mathbf{A} \mathbf{x}^k \mathbf{b}).$ 5: $\mathbf{w} \leftarrow S \mathbf{x}^k.$
- 6

for each
$$i \in \{1, 2, \dots, n^2\}$$
 do

$$y_i^{k+1} \leftarrow x_i^k - \frac{v_i + \alpha \cdot w_i + \mu \cdot G_{0,\sigma}(v_i) \cdot \nabla g_{\rho}(x_i^k)}{\lambda + \mu}$$

$$x_i^{k+1} \leftarrow \begin{cases} l_1, & \text{if } y_i^{k+1} < l_1, \\ y_i^{k+1}, & \text{if } l_1 \le y_i^{k+1} \le l_c, \\ l_c, & \text{if } l_c < y_i^{k+1}. \end{cases}$$
end for

9. end for

10:
$$k \leftarrow k+1$$

- 11: **until** a stopping criterium is met.
- 12: Apply a discretization of \mathbf{x}^k to gain fully discrete results.

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Description of the iteration

$$y_i^{k+1} \leftarrow x_i^k - \frac{v_i + \alpha \cdot w_i + \mu \cdot G_{0,\sigma}(v_i) \cdot \nabla g_p(x_i^k)}{\lambda + \mu}$$

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Description of the iteration

 $\frac{v_i + \alpha \cdot w_i + \mu \cdot G_{0,\sigma}(v_i) \cdot \nabla g_p(x_i^k)}{\lambda + \mu}$ x_i^{κ} previous iteration step

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Description of the iteration

 $v_i + \alpha \cdot w_i + \mu \cdot G_{0,\sigma}(v_i) \cdot \nabla g_p(x_i^k)$ x_i^{κ} $\lambda + \mu$ previous iteration step smoothness term

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Results of the optimization

The result of the optimization process is a semi-continuous reconstruction on which pixel values are somewhat steered towards discrete solutions.







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Example of the process

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Evaluation of the algorithm

We evaluated the algorithm by running software tests.

- We have chosen two other reconstruction algorithms for comparision.
 - Discrete Algebraic Reconstrction Algorithm (DART)

K.J. Batenburg, J. Sijbers, DART: a practical reconstruction algorithm for discrete tomography. IEEE Transactions on Image Processing 20(9), pp. 2542–2553 (2011).

• A D.C. programming based algorithm, that is capable of reconstructing binary images by minimizing an energy function. (DC)

T. Schüle, C. Schnörr, S. Weber, J. Hornegger, *Discrete tomography by convex-concave regularization and D.C. programming*, Discrete Applied Mathematics 151, pp. 229–243 (2005).

- We reconstructed a set of software phantoms from their projections with the three given algorithms.
- After the reconstructions we compared the results for evaluation.

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Original image



DC, 5 projs.



DART, 5 projs.



Prop. method, 5 projs.







DART, 6 projs.



Prop. method, 6 projs.

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Original image



DART, 6 projs.



Prop. method, 6 projs.



DC, 9 projs.



Prop. method, 9 projs.

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Original image



DART, 15 projs.



Prop. method, 15 projs.



DC, 18 projs.



Prop. method, 18 projs.

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Numerical results

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	DC		DART		Prop. method	
projections	Error	Time	Error	Time	Error	Time
2	90.7%	12.1 s.	85.6 %	6.6 s.	107.4%	10.1 s.
3	22.0%	12.4 s.	52.9%	5.4 s.	30.8%	11.2 s.
4	1.2%	13.6 s.	44.9%	8.0 s.	22.4%	11.8 s.
5	0.3%	12.5 s.	29.9%	9.5 s.	7.9%	12.7 s.
6	0.2%	8.1 s.	0.2%	2.7 s.	0.8%	7.6 s.
9	0.2%	6.5 s.	0.0%	0.8 s.	0.3%	4.6 s.
12	0.0%	7.2 s.	0.0%	0.9 s.	0.1%	4.8 s.
15	0.0%	8.7 s.	0.0%	1.2 s.	0.1%	5.8 s.
18	0.0%	8.7 s.	0.0%	0.9 s.	0.1%	5.8 s.

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	DC		DART		Prop. method	
projections	Error	Time	Error	Time	Error	Time
2	-	-	62.9%	6.7 s.	52.7%	10.4 s.
3	-	-	45.1%	8.0 s.	41.9%	11.4 s.
4	-	-	43.4%	8.6 s.	35.4%	12.2 s.
5	-	-	36.4%	9.4 s.	26.4%	13.2 s.
6	-	-	27.0%	10.2 s.	11.6%	13.8 s.
9	-	-	0.7%	4.5 s.	1.9%	15.6 s.
12	-	-	0.4%	14.9 s.	1.0%	11.6 s.
15	-	-	0.3%	2.3 s.	0.8%	11.6 s.
18	-	-	0.1%	21.3 s.	0.6%	10.9 s.

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	DC		DART		Prop. method	
projections	Error	Time	Error	Time	Error	Time
2	-	-	84.4%	6.7 s.	85.7%	9.3 s.
3	-	-	77.3%	8.2 s.	82.5%	6.0 s.
4	-	-	75.3%	8.8 s.	81.0%	8.0 s.
5	-	-	73.3%	9.7 s.	74.2%	10.2 s.
6	-	-	74.1%	10.2 s.	70.0%	12.7 s.
9	-	-	57.0%	12.6 s.	46.8%	14.7 s.
12	-	-	33.9%	14.5 s.	24.8%	11.4 s.
15	-	-	22.0%	18.0 s.	16.3%	8.6 s.
18	-	-	15.7%	20.8 s.	14.0%	8.0 s.

Summary

Tomography László Varga, Péter Balázs, Antal Nagy

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Reconstruction Algorithm for Multivalued Discrete

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- Based on the results, the proposed method can compete with the other two algorithms in both speed and accuracy of the results.
- With reconstructions of images containing at least 3 intensity levels from few projections, it could outperform the other two methods.
- There are several possible ways for improvement and alternative applications of the algorithm.

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